

SEGMENTATION OF TEXTURED IMAGES USING NETWORK OF SYNCHRONISED OSCILATORS

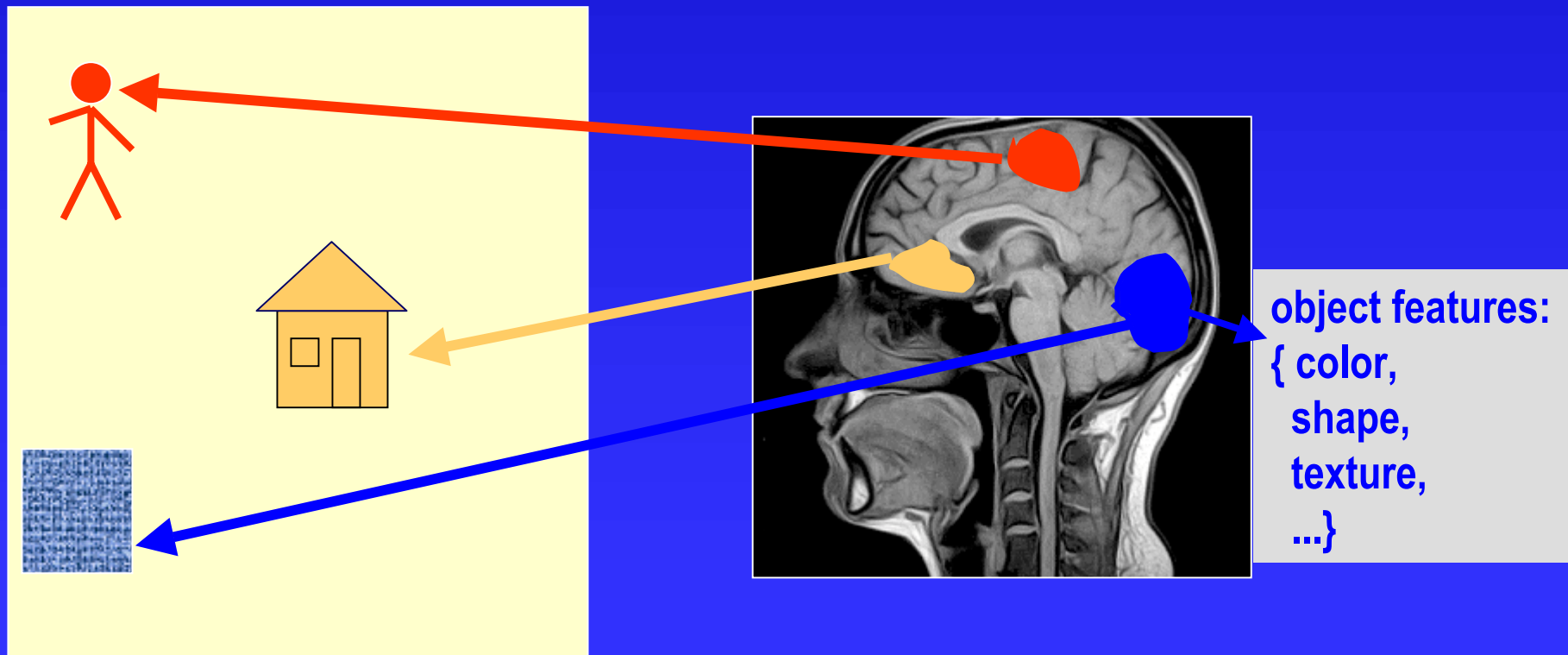
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COST B11, 2-4 MAY 2002, BERGEN

„Temporary correlation” theory (von der Malsburg, 1981) tries to explain how the image scene segmentation is performed by human brain.



The network of synchronous oscillators (Wang & Teman 1995, Linsay & Wang 1998)

LEGION - Locally Excitatory Globally Inhibitory Oscillator Network

- **network of locally connected oscillators, each image point is represented by one oscillator**
- **oscillators connected to a given object are simultaneously synchronised**
- **other oscillators are disabled**
- **after same time active synchronised oscillators are desynchronised, while the other oscillator group starts synchronisation (this group represents a different object)**

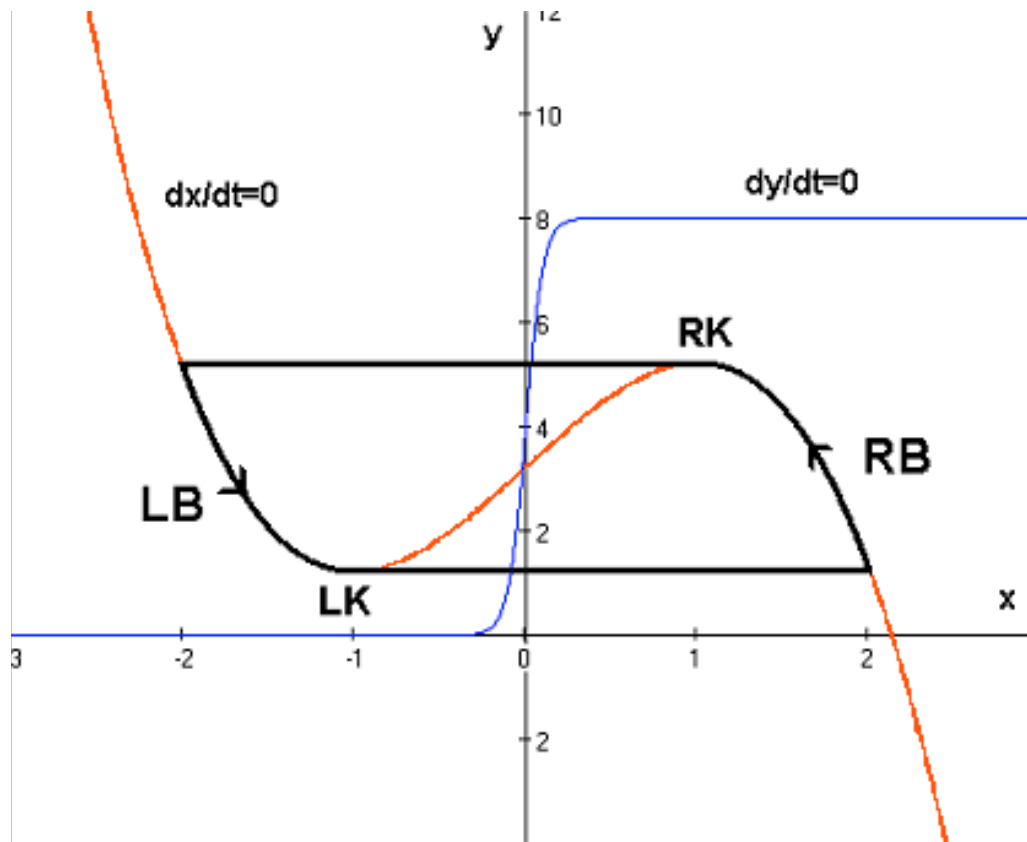
The mathematical model of single oscillator

x - excitatory variable, y - inhibitory variable

$$\begin{aligned}\frac{dx}{dt} &= 3x - x^3 + 2 - y + I_T \\ \frac{dy}{dt} &= \varepsilon \left\{ \gamma \left[1 + \tanh\left(\frac{x}{\beta}\right) \right] - y \right\}\end{aligned}$$

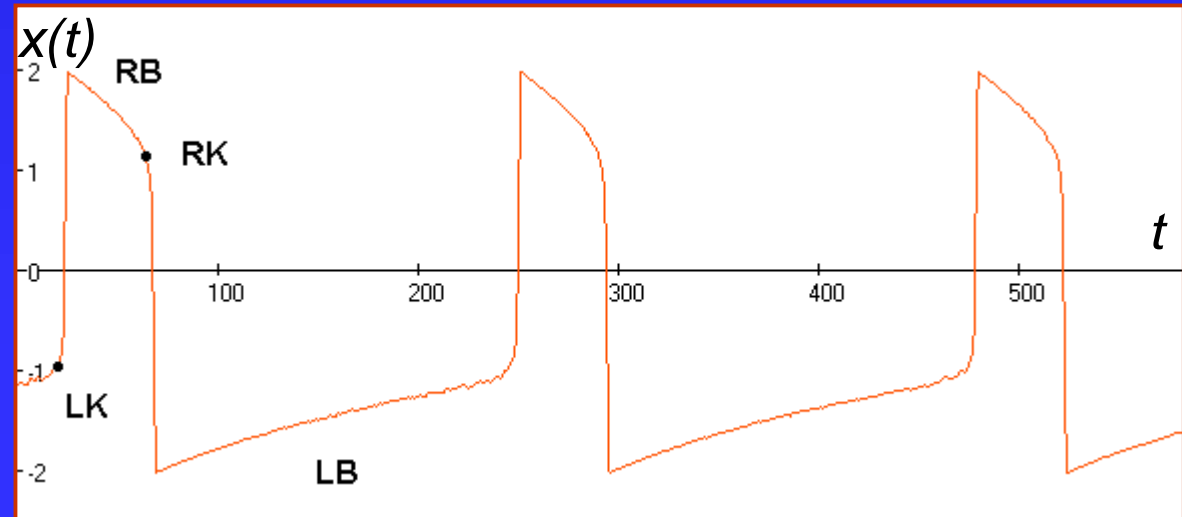
I_T - excitation of oscillator x :

$I_T > 0$ - activated (oscillatory), $I_T \leq 0$ - disabled

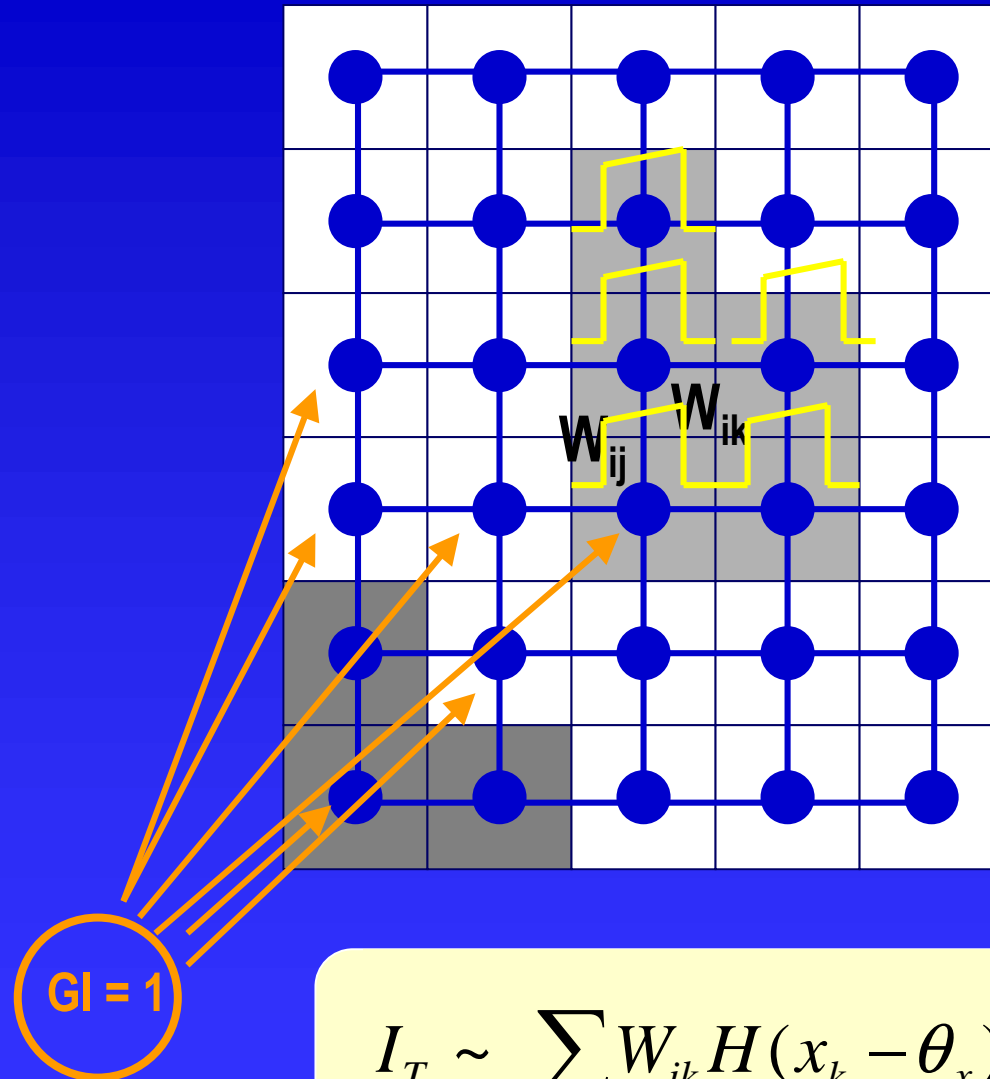


Nullclines ($dx/dt=0$, $dy/dt=0$)
and trajectory of an oscillator x

The output waveform
 $x(t)$ of an oscillator x



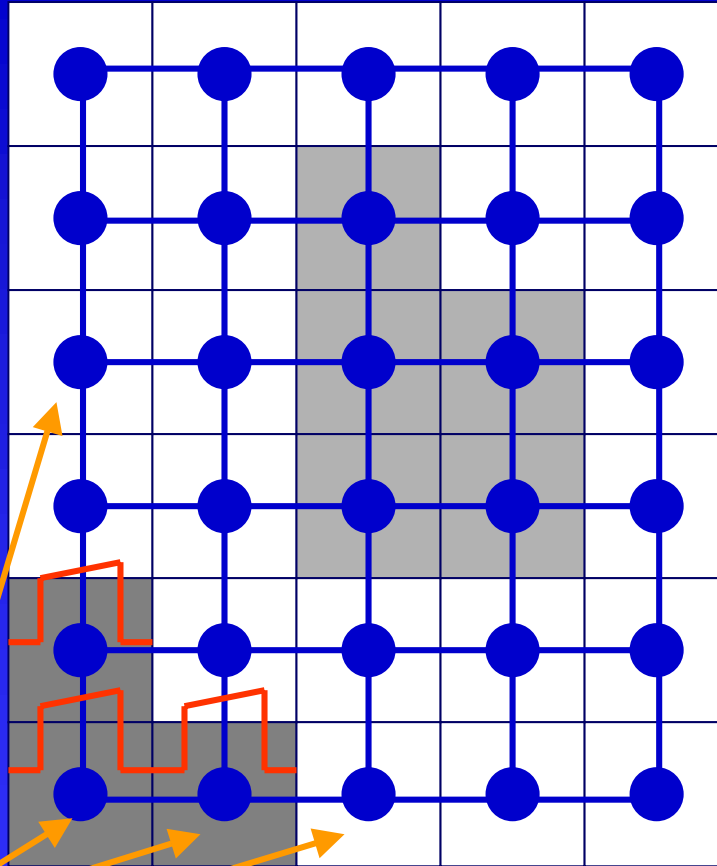
The network of locally connected oscillators



GI - global inhibitor,
equal to 1 when
at least one oscillator
is activated
and 0 otherwise

$$I_T \sim \sum_{k \in N(i)} W_{ik} H(x_k - \theta_x) - GI \cdot W_z \quad H(t) = \begin{cases} 0, & t < 0 \\ 1, & t \geq 0 \end{cases}$$

The network of locally connected oscillators

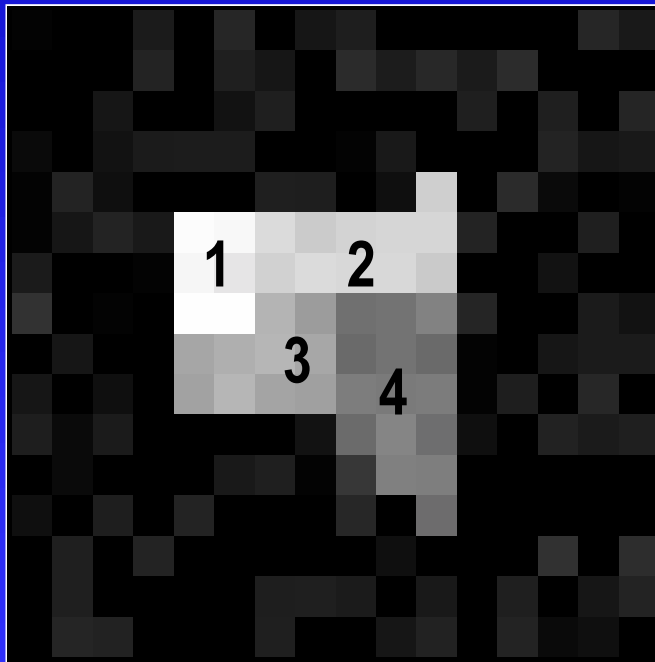


GI=1

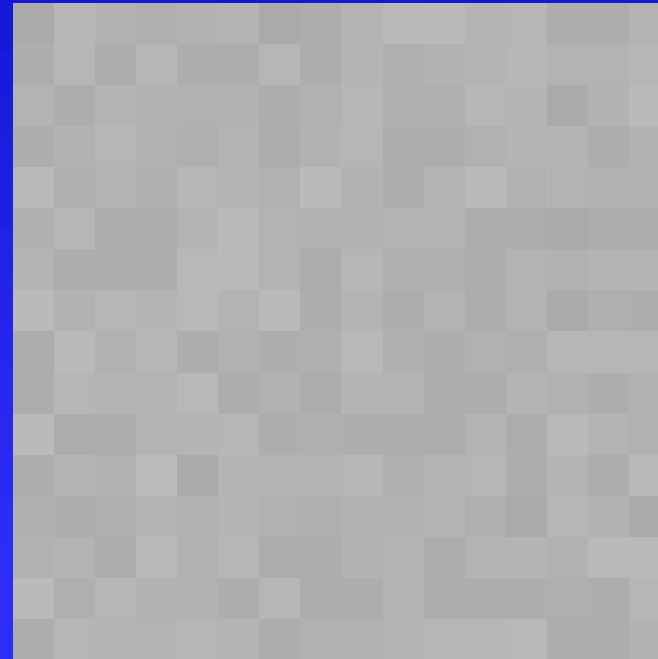
$$I_T \sim \sum_{k \in N(i)} W_{ik} H(x_k - \theta_x) - GI \cdot W_z \quad H(t) = \begin{cases} 0, & t < 0 \\ 1, & t \geq 0 \end{cases}$$

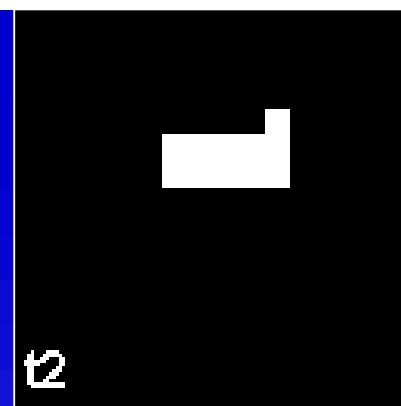
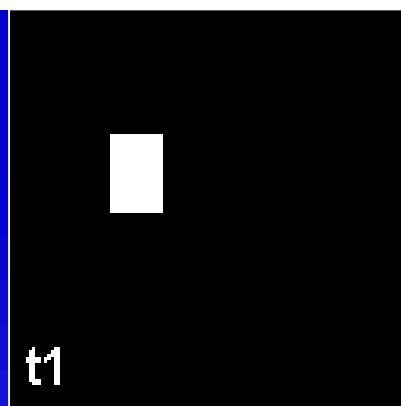
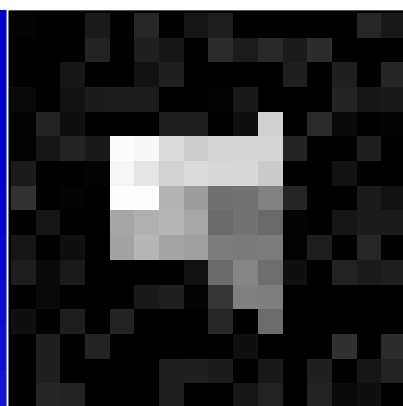
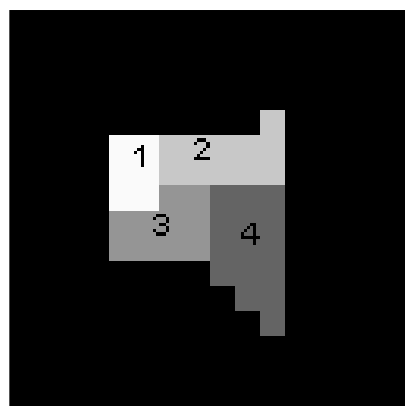
Example of grey-level image segmentation corrupted by Gaussian noise

16×16

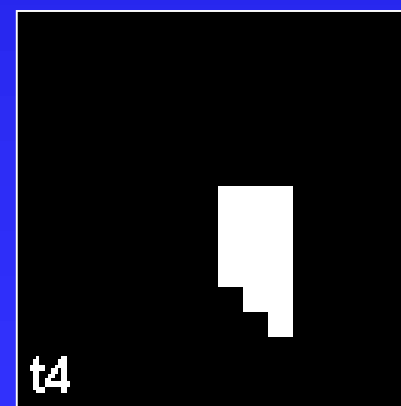
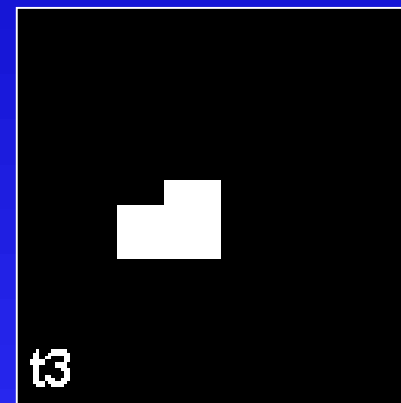
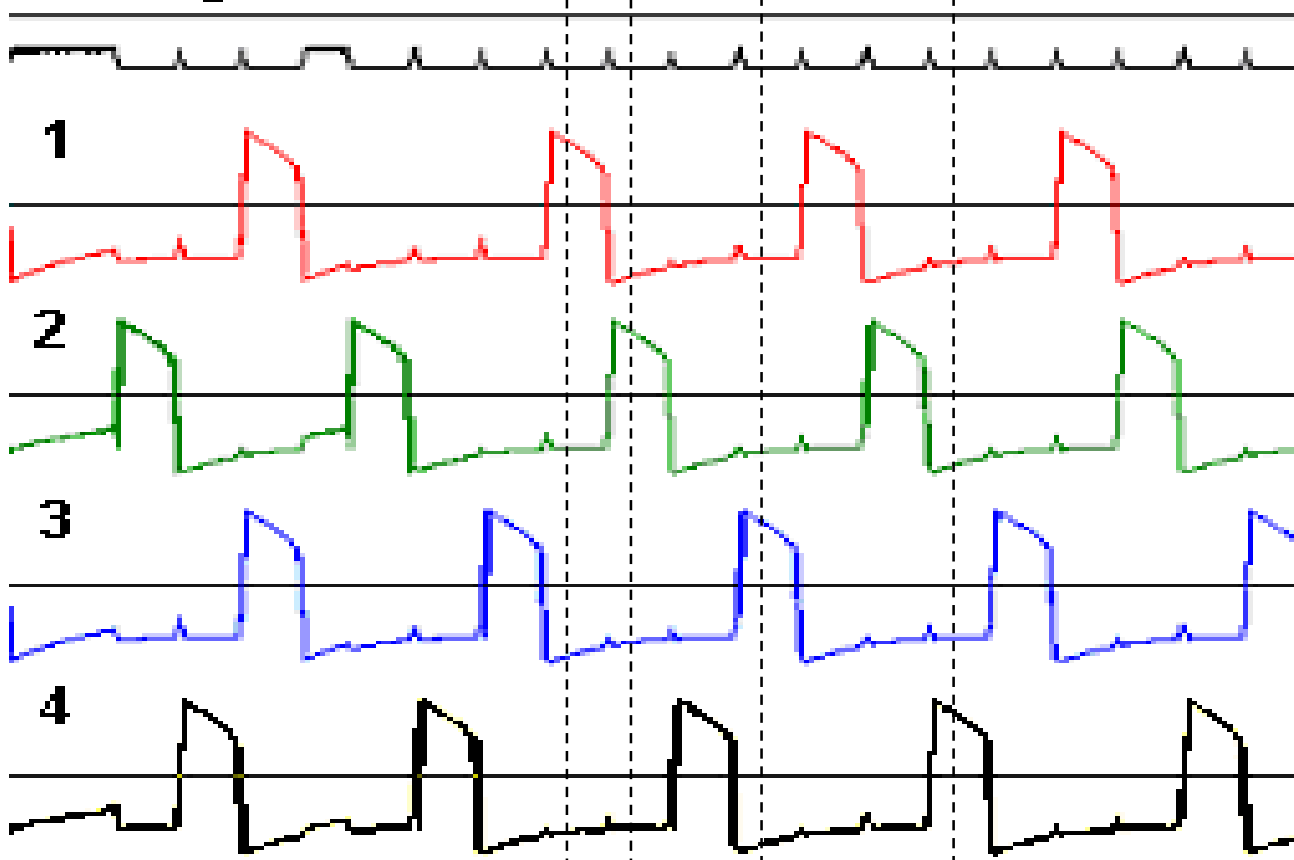


iterations



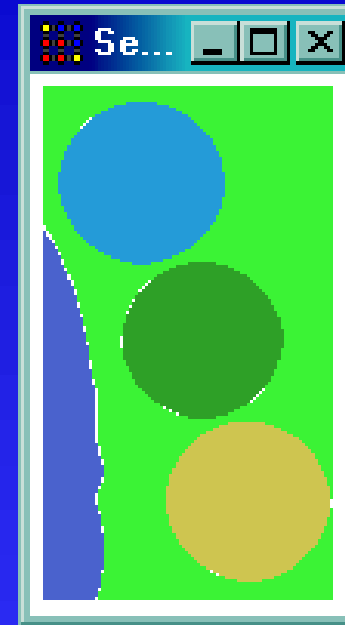
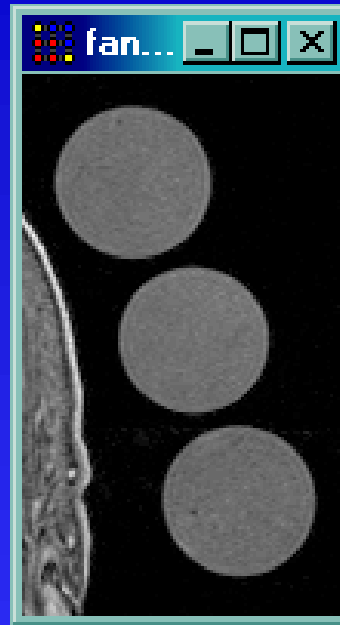


background



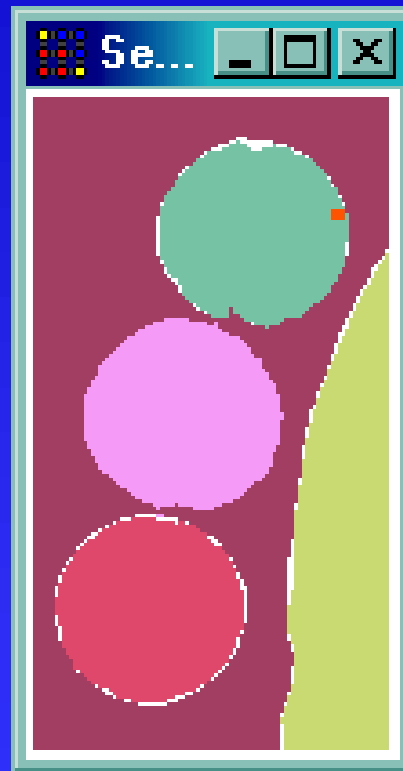
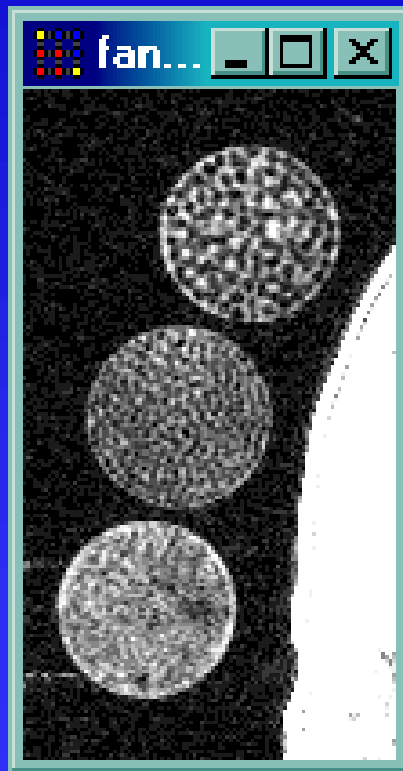
Example of MRI image segmentation

Foam phantoms



To speed up calculation in the network, it is possible to apply an algorithm, where simplified oscillator model is assumed (Linsay & Wang 1998)

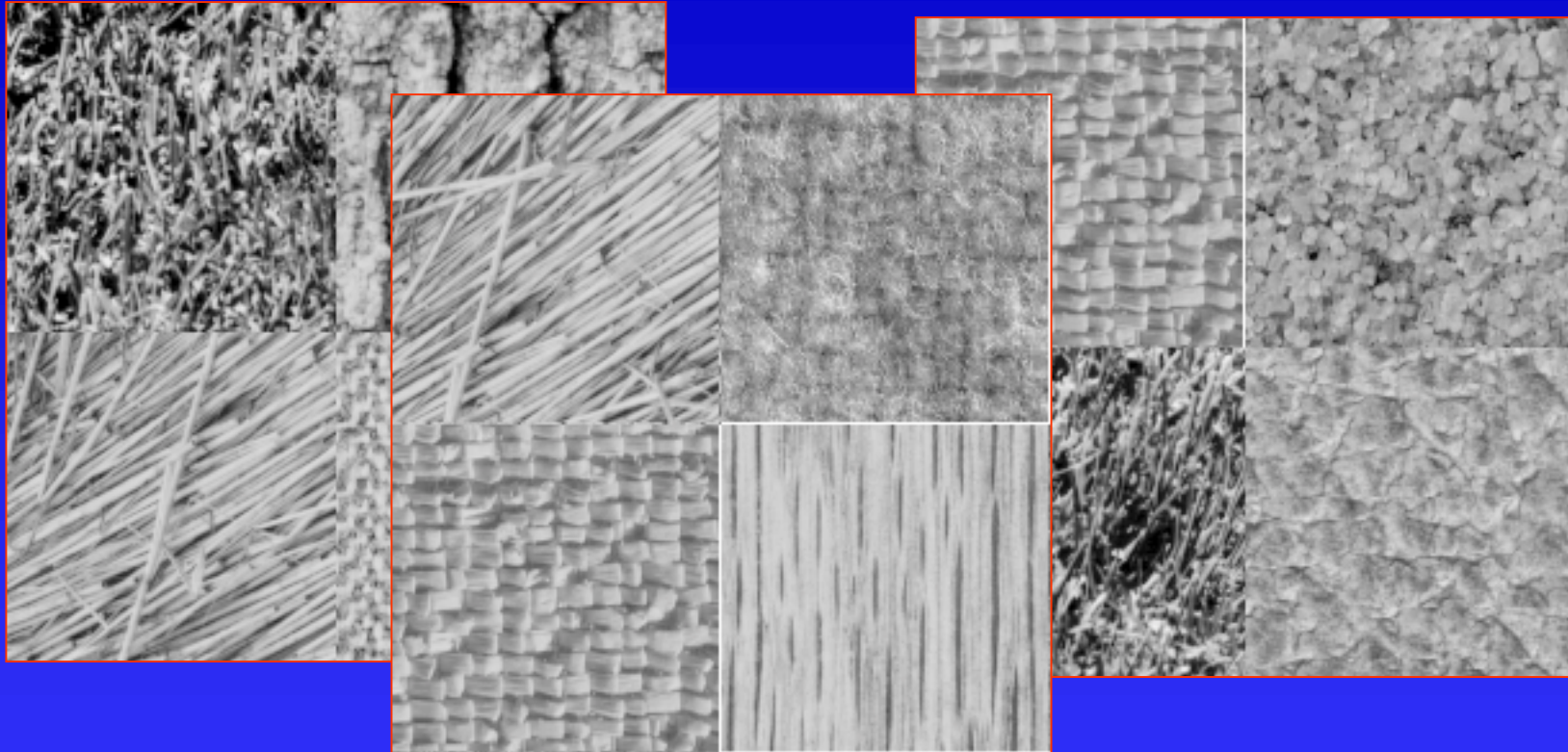
Example of MRI image segmentation



PS phantoms

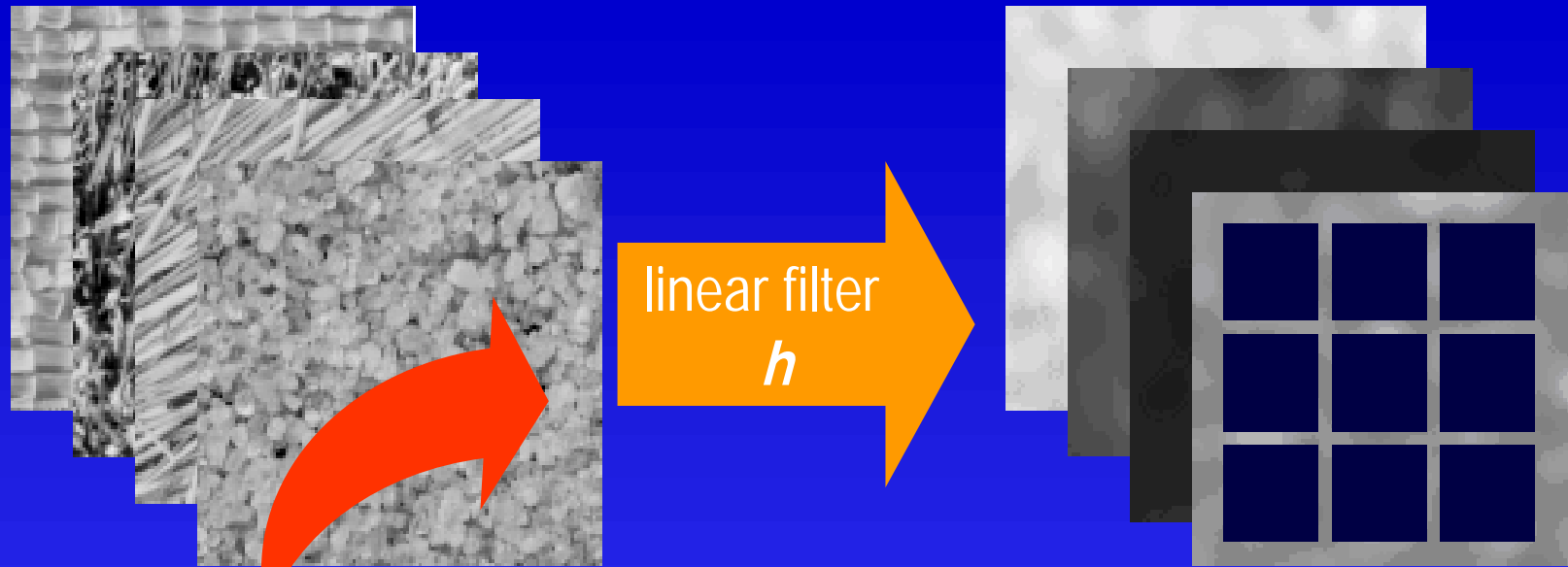
$$W_{ij} = \frac{U_{\max}}{1 + |U_i - U_j|} \quad U_i - \text{median in } 5 \times 5 \text{ window}$$

Segmentation of textured images



There is a need to find texture features which are able to segment analysed images. These features will be used to form oscillator weights.

Features based on linear optimised filtering



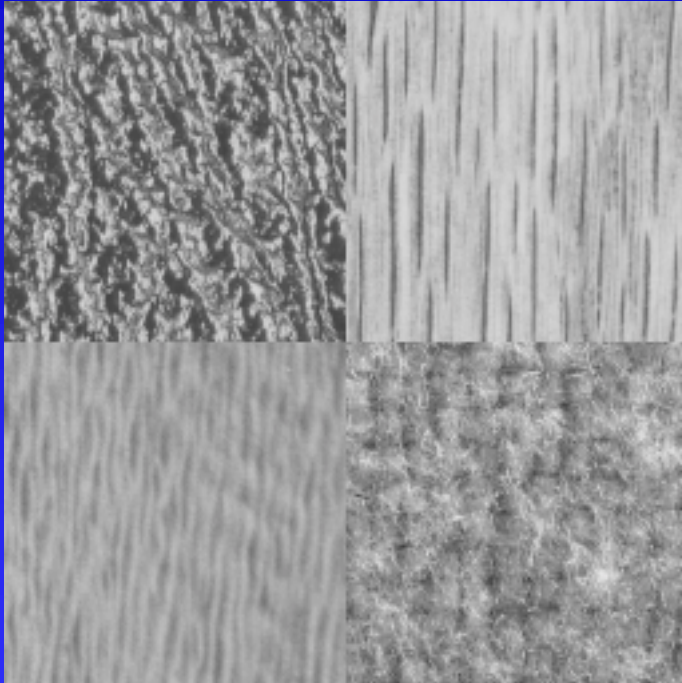
optimisation of h
to increase F

feature
extraction

estimation of mean and
variance for these
features

$$F(h) = \frac{D^2}{V^2} = \frac{\frac{1}{K-1} \sum_{k=1}^K \sum_{j=1}^K |\mu_k - \mu_j|^2}{\sum_{k=1}^K V_k^2}$$

Segmentation example



sample texture from
Brodatz album

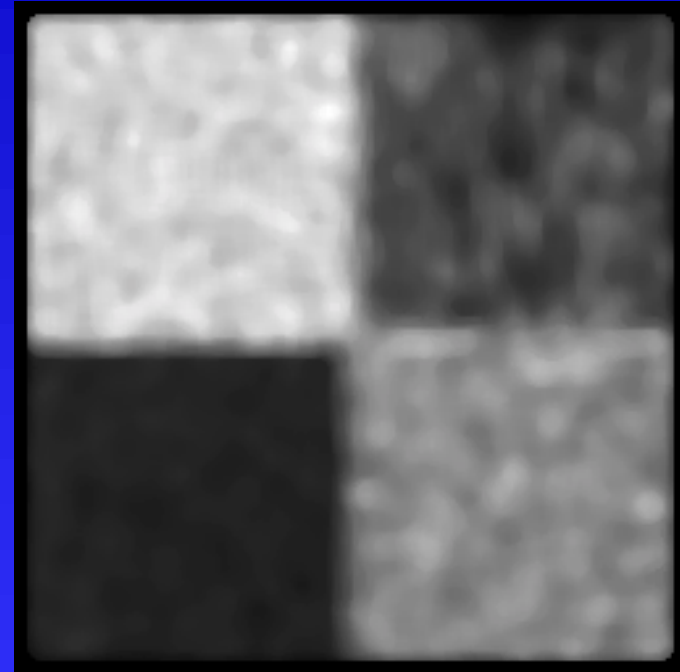
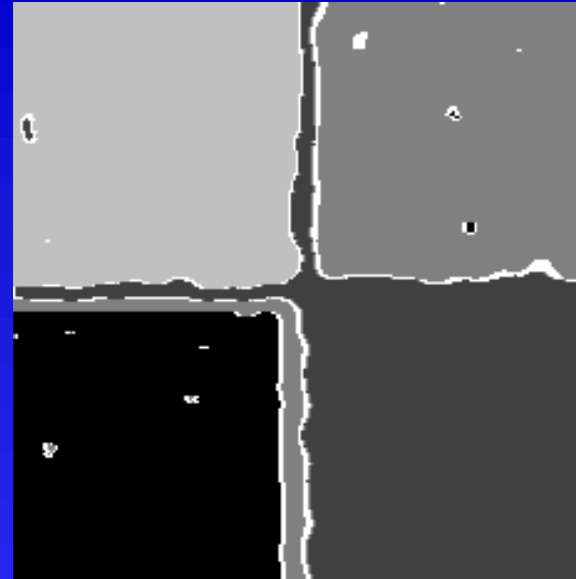


image after filtering, 7x7

Comparison of different segmentation methods



LEGION



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region
growing

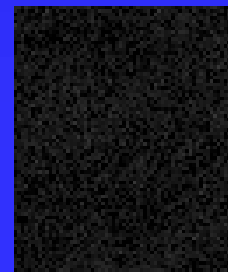
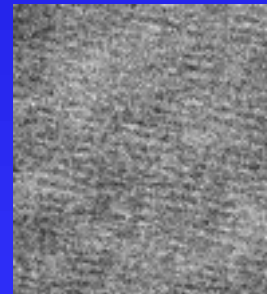
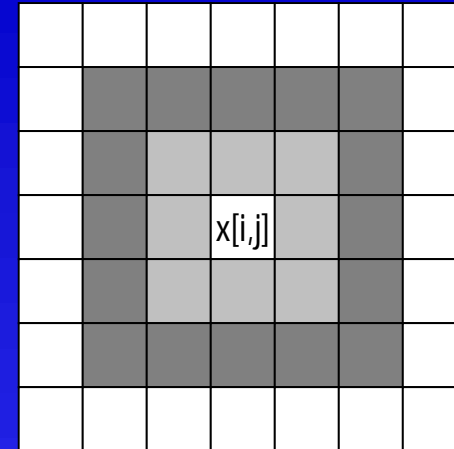


thresholding

Features based on Gaussian Markov random field model

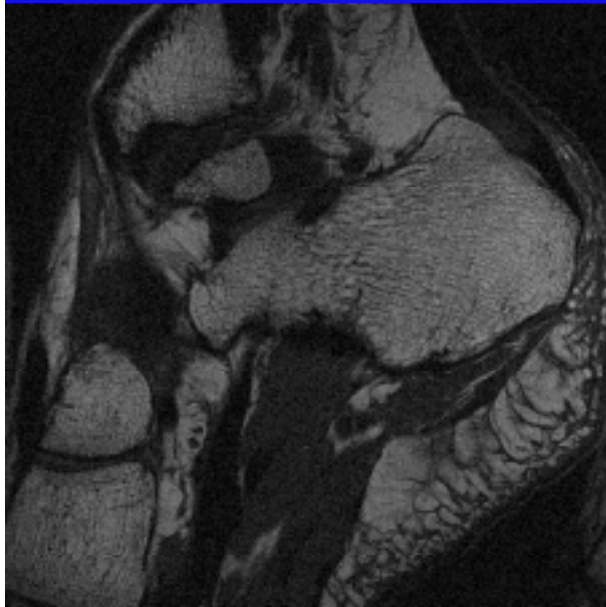
$$X[i, j] = \sum_{(k, l) \in N_v} \theta_{k, l} X[i + k, j + l] + e[i, j]$$

MRI crossection of human foot (Heidelberg)



artificial textures
generated based on
estimated GMRF
parameters

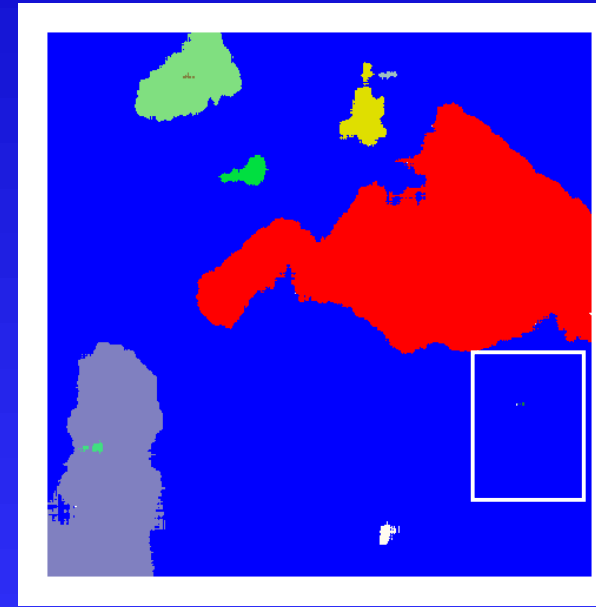
Segmentation example of MRI textured image



original image



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LEGION

Conclusions

Presented image segmentation method that uses LEGION provides promising results for a sample MRI textured images.

The most important problem is to find appropriate texture features. The features based on optimised linear filters and GMRF model are suitable for classification of analysed textures.

The LEGION may be realised in VLSI chip, which would provide parallel image segmentation.